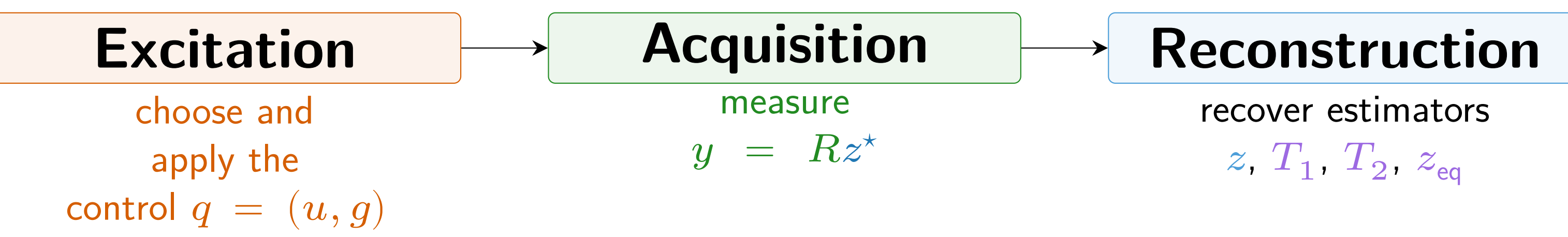


Motivation (Bloch-Torrey equation for MRI)

State: z^* (magnetisation), control $q(t) = (u(t), g(t))$ with radio-frequency pulses $u(t)$ and gradients $g(t)$, parameters T_1^* , T_2^* , z_{eq}^* .

$$\partial_t z^* + \gamma z^* \times \underbrace{\begin{pmatrix} u_x(t) \\ u_y(t) \\ B_0 + g(t) \end{pmatrix}}_{\text{excitation}} - \underbrace{D \Delta z^*}_{\text{diffusion}} + \underbrace{\text{diag}\left(\frac{1}{T_2^*}, \frac{1}{T_2^*}, \frac{1}{T_1^*}\right)}_{\text{relaxation}} z^* = \begin{pmatrix} 0 \\ 0 \\ z_{eq}^*/T_1^* \end{pmatrix}.$$



Abstract framework & objectives

Main equation:

$$\partial_t z^* + [H_0(z^*) - H_1]\theta^* + [C_0(q) - C_1]z^* = 0.$$

Partial state observation:

$$y = Rz^*.$$

Objectives:

- reconstruct both state $z^*(t)$ and parameter θ^* ,
- do so quickly and precisely,
- design a control q optimising the reconstruction.

Online parameter estimation

Estimators z of z^* and $\theta(t)$ of θ^* :

$$\begin{aligned} \partial_t z + [H_0(z) - H_1]\theta + [C_0(q) - C_1]z &= \Psi^z(z, \theta, y), \\ \partial_t \theta &= \Psi^\theta(z, \theta, y). \end{aligned}$$

Advantages:

- reconstruction starts during acquisition (quicker feedback),
- enables observation-based controls $q(t, x, y)$.

State of the art:

- Adaptive Lyapunov – Persistence of Excitation methods: [1, 3, 4].
- Partial-observation online estimators: [3, 4].
- Nonlinear inverse and input-design approaches: [2, 5, 6].

Estimator construction

Estimators $z^\perp$ (of $z^* - R^\dagger y$) and θ (of θ^*):

$$\begin{cases} \bar{z} = R^\dagger y + z^\perp, \\ \partial_t z^\perp + R^\perp (H_0(\bar{z})\theta + C_0(q)\bar{z}) = \Psi^\perp, \\ \partial_t \theta = \Psi^\theta. \end{cases}$$

Differentiate the observation:

$$\partial_t y = R \partial_t z^* = -R([H_0(z^*) - H_1]\theta^* + [C_0(q) - C_1]z^*),$$

obtaining the new observable residual $r = R \partial_t \bar{z} - \partial_t y$ satisfying

$$r = R([H_0(\bar{z}) - H_1](\theta - \theta^*) + [\tilde{H}_0(\theta^*) + C_0(q) - C_1](\bar{z} - z^*)).$$

Hypotheses

- Regularity hypotheses** on H_0 , H_1 , C_0 , C_1 : guarantee well-posedness of equations and estimators.
- Initial error smallness**: necessary condition for estimator convergence for nonlinear systems
- Persistence of excitation**, to guarantee that the parameter is identifiable: for a given control q , there exist $\tau > 0$ and $\varepsilon > 0$ such that for all $T > 0$,

$$\int_T^{T+\tau} \|r\|^2 dt \geq \varepsilon_q \|\theta - \theta^*\|^2.$$

Results

Proposition

For a gain $\mu(t) > 0$ large enough, choose

$$\begin{cases} \Psi^\perp = -\mu [\tilde{H}_0(\theta) + C_0(q) - C_1]^* r, \\ \Psi^\theta = -\mu [H_0(\bar{z}) - H_1]^* r. \end{cases}$$

Under aforementioned hypotheses, we obtain $0 < \alpha < 1$, such that for all $t > 0$

$$\|\theta(t+T) - \theta^*\|^2 \leq \alpha \|\theta(t) - \theta^*\|^2.$$

Toy numerical example

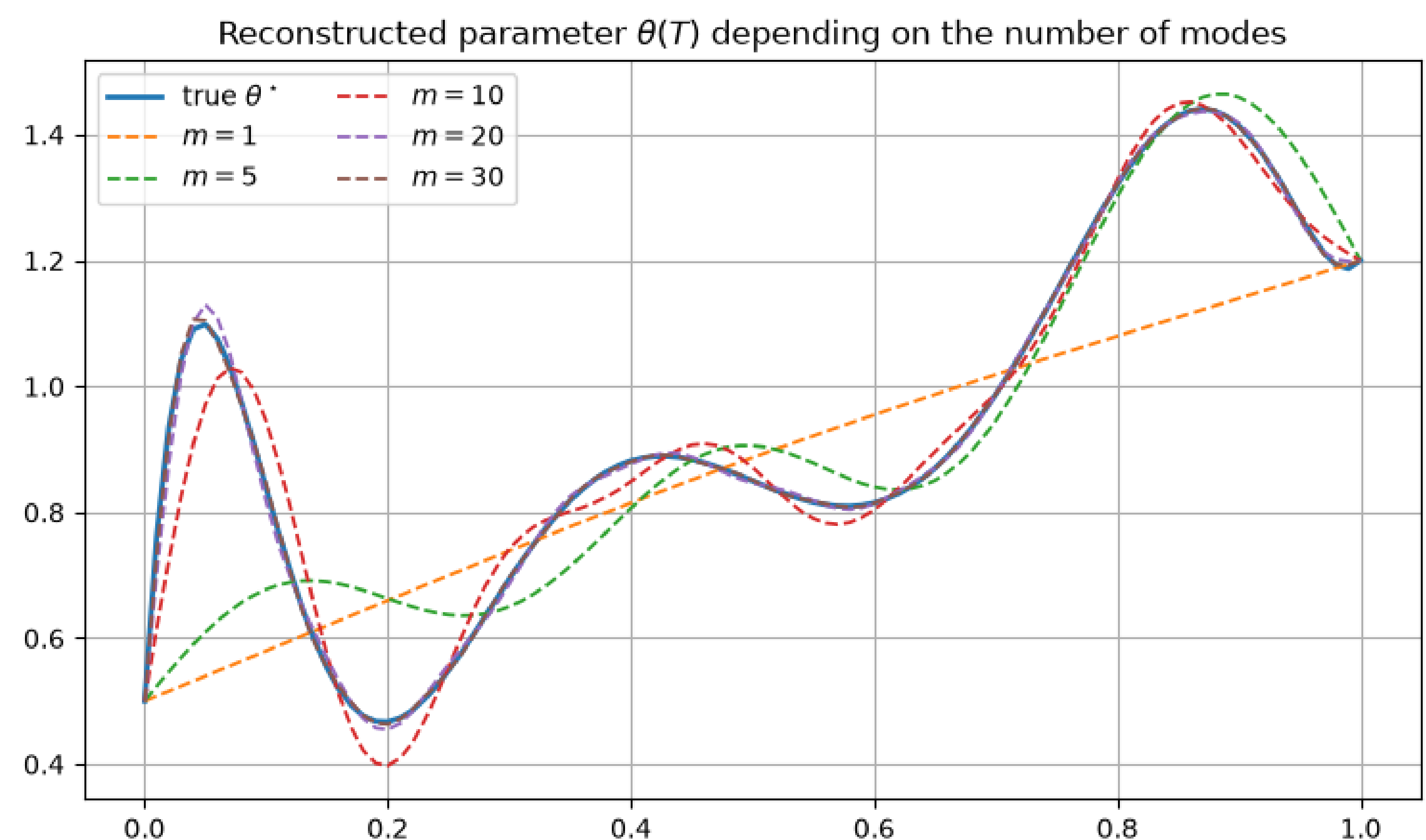
Uncontrolled 1D heat-equation:

$$\begin{cases} \partial_t z^* - \Delta z^* + \theta^* z^* = b z^* & \text{on } (0, 1), \\ z^* = 0 & \text{on } \{0, 1\}, \end{cases}$$

with spectral partial observation:

$$y = 2 \sum_{k=1}^m \langle \sin(k\pi \cdot), z^* \rangle \sin(k\pi \cdot)$$

and knowledge of $\theta^*(0)$ and $\theta^*(1)$. For $T = 1$ and $\mu(t) = 10$, convergence is partial and depends on the number of modes:



Outlook

How should one choose the control to optimise the reconstruction?

- maximise the associated observability constant,
- consider open-loop vs. observation-dependent controls.

Jointly, can one lessen the persistence of excitation condition to make it estimator-independent?

References

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